



Contents lists available at ScienceDirect

Clinical Oncology

journal homepage: www.clinicaloncologyonline.net

Adaptive Radiotherapy Enabled by MRI Guidance

A. Hunt ^{*†}, V.N. Hansen ^{*‡}, U. Oelfke ^{*‡}, S. Nill ^{*‡}, S. Hafeez ^{*†}^{*}The Institute of Cancer Research, London, UK[†]The Royal Marsden NHS Foundation Trust, London, UK[‡]Joint Department of Physics, The Royal Marsden NHS Foundation Trust, London, UK

Received 2 August 2018; received in revised form 10 August 2018; accepted 20 August 2018

Abstract

Adaptive radiotherapy (ART) strategies systematically monitor variations in target and neighbouring structures to inform treatment-plan modification during radiotherapy. This is necessary because a single plan designed before treatment is insufficient to capture the actual dose delivered to the target and adjacent critical structures during the course of radiotherapy. Magnetic resonance imaging (MRI) provides superior soft-tissue image contrast over current standard X-ray-based technologies without additional radiation exposure. With integrated MRI and radiotherapy platforms permitting motion monitoring during treatment delivery, it is possible that adaption can be informed by real-time anatomical imaging. This allows greater treatment accuracy in terms of dose delivered to target with smaller, individualised treatment margins. The use of functional MRI sequences would permit ART to be informed by imaging biomarkers, so allowing both personalised geometric and biological adaption. In this review, we discuss ART solutions enabled by MRI guidance and its potential gains for our patients across tumour types.

© 2018 The Royal College of Radiologists. Published by Elsevier Ltd. This is an open access article under the CC BY-NC-ND license (<http://creativecommons.org/licenses/by-nc-nd/4.0/>).

Key words: Adaptive radiotherapy; gating; image guided; magnetic resonance imaging; radiotherapy planning; tracking

Search Strategy and Selection Criteria

An electronic literature search was carried out using PubMed and Web of Science databases. The final search was carried out in July 2018. Search terms included “radiotherapy”, “radiotherapy planning”, “adaptive radiotherapy”, “online adaptive radiotherapy”, “magnetic resonance”, “MR”, “MR-guided”, “radiotherapy tracking”, and “radiotherapy gating”. The search was restricted to those published in English with preference given to more recent studies. Selected studies were first screened by their title and/or abstract followed by full article review of relevant articles. A manual review of the reference list of relevant studies was also undertaken.

Introduction

The target for radiotherapy is dynamic. It varies in position, shape, size, and biology over a time frame that extends

over seconds, days, and weeks (Figure 1). Reliance on a single pre-treatment planning computed tomography (CT) scan to capture this change over the treatment course is misplaced. Historically, to try and account for this geometric variation, large margins have been used to create the planning target volume (PTV) [1–3]. This, however, often limits dose escalation to tumoricidal levels because of concerns regarding collateral damage to adjacent normal structures [4,5].

Accepting that the PTV is a statistical construct to ensure that dose can be successfully delivered to the tumour, reliably decreasing PTV size is only possible when there is confidence in target positioning during treatment. Technologies that have enabled imaging in the treatment room have allowed gains to be made on this front, so overcoming, in part, the challenge of hitting an otherwise invisible target with an invisible beam. Image-guided radiotherapies (IGRTs), particularly those permitting soft-tissue visualisation, such as cone-beam CT (CBCT), prior to treatment delivery, have already demonstrated step-wise improvement in target coverage. This has been achieved using smaller margins and a subsequent reduction in integral

Author for correspondence: S. Hafeez, Royal Marsden Hospital, Downs Road, Sutton, Surrey SM2 5PT, UK. Tel.: 0208 661 3467.

E-mail address: shaista.hafeez@icr.ac.uk (S. Hafeez).

<https://doi.org/10.1016/j.clon.2018.08.001>

0936-6555/© 2018 The Royal College of Radiologists. Published by Elsevier Ltd. This is an open access article under the CC BY-NC-ND license (<http://creativecommons.org/licenses/by-nc-nd/4.0/>).

Please cite this article in press as: Hunt A, et al., Adaptive Radiotherapy Enabled by MRI Guidance, Clinical Oncology (2018), <https://doi.org/10.1016/j.clon.2018.08.001>

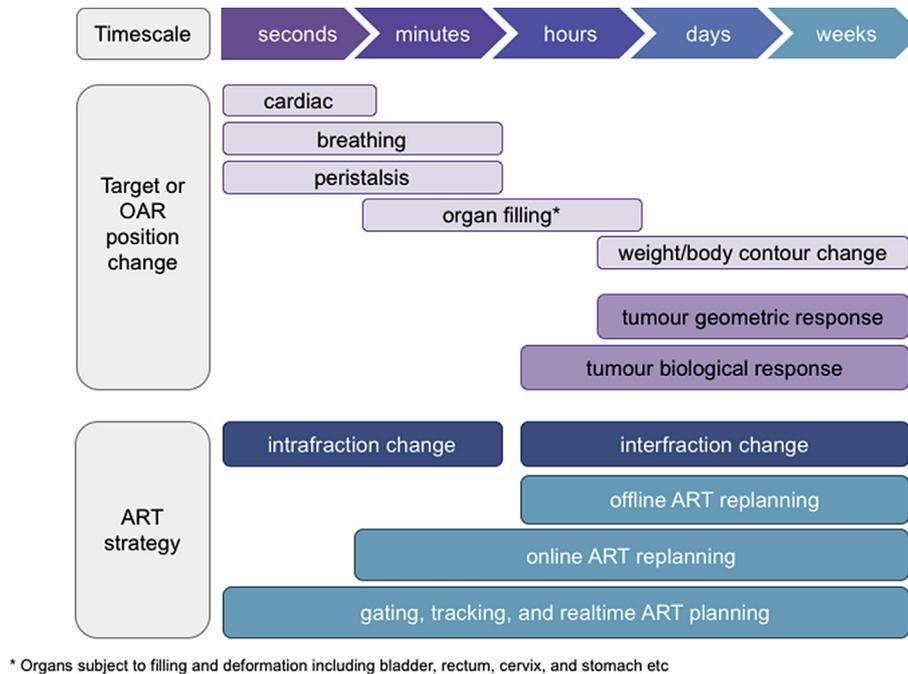


Fig 1. Timescales for adaptation and ART solutions implemented .

dose to surrounding tissues when compared to surrogates for target position such as skin tattoos or bony anatomy [6].

Adaptive radiotherapy (ART) is an umbrella term encompassing techniques that allow knowledge of patient-specific anatomical variations informed by IGRT to feedback into the plan and dose-delivery optimisation during the treatment course [7]. This ensures that the planned dose is delivered as accurately and precisely as possible according to the anatomy of the day. ART can be implemented broadly over three timescales (Figure 1): (1) offline between fractions, (2) online immediately prior to a fraction, and (3) in real-time during a fraction.

Offline ART monitors the position of the target during a limited number of fractions. It addresses systematic changes to some extent, but also allows opportunity for an individualised PTV margin to be applied based on acquired knowledge of the location of volumes of interest and patient set-up. Although adaptation is not informed by the exact position of the tumour at each fraction, the applied margins are often smaller than population derived margin recipes [8,9]. Online and real-time ART protocols modify the treatment plan while the patient remains on the couch. These strategies allow for a patient specific PTV to be created because they are informed by the actual change in anatomy seen for that fraction. As there is greater certainty to the true position of the tumour, an even smaller “safety” margin can be considered. The confidence in soft-tissue targeting at the time of radiotherapy delivery provides an opportunity to deliver higher radiation doses with tighter margins. In this review, we discuss ART solutions enabled by magnetic resonance imaging (MRI) guidance and its potential gains for our patients.

Will MRI-Guided Radiotherapy be the Ultimate Online IGRT Solution?

The persisting weakest link in the treatment chain for radiotherapy remains clinician-led target identification [10,11]. Repeated studies have demonstrated that gross tumour volume (GTV) and organ at risk (OARs) delineation variability between observers introduces systematic errors, which are larger than daily set-up uncertainties [12–14].

One of the most important factors responsible for the observed target variation is adequate imaging [12]. Compared to CT or CBCT, MRI offers superior soft-tissue definition with no associated radiation risk [15–17]. As a result, for many tumours diagnostic MRI improves inter- and intra-observer delineation consistency [12,18–20]. Observer variation also improves with the use of standardised guidelines, anatomy atlases, and auto-segmentation tools [21].

MRI delineated target volumes are often reported to be significantly different from those contoured on CT. Occasionally, MRI identifies targets larger than on CT because tumour that otherwise would have been missed is now seen [20]; however, most commonly, targets are reported to be smaller when delineated on MRI [18,19,22,23]. The resulting smaller MRI-derived target improves the therapeutic ratio so enabling dose escalation. For example, an MRI-delineated prostate, allows dose escalation of 2–7 Gy while maintaining the same rectal wall dose compared with a CT-delineated prostate [24]. Similarly, in cervical cancer, dose escalation is possible using an MRI-informed target with an associated 10–20% survival gain seen at 3 years with reduced gastrointestinal and urinary late morbidity [25].

It is likely that MRI-guided IGRT will help define the 'right' radiotherapy target, but robust pathological correlation is necessary as the GTV is a factual construct of macroscopic disease. Only with this information will it be possible to know how closely the MRI visualised target represents the 'true' pathological target and how closely the delineated GTV represents actual disease [2]. Without this knowledge, although ART targets may get progressively smaller, and dose more conformal, we risk possible increases in marginal recurrences, undoing all efforts invested in improving radiotherapy precision and accuracy with this technology [26,27].

The availability of on-board 'functional' MRI sequences holds promise that geometric adaptation maybe complemented by biological adaptation. For example, diffusion-weighted imaging (DWI) is a functional imaging technique dependent on the inhibitory effect of cell membranes to the random motion of water molecules to generate image contrast. As tumours usually have greater cellularity than normal tissue, they demonstrate higher signal intensity, i.e., restricted diffusion on MRI. This is reflected in the low mean apparent diffusion coefficient (ADC) value. This has potential to provide both qualitative and quantitative information. Change in the ADC has been used to identify early treatment response, and to predict local recurrence [28–30]. Therefore, on-board DWI could identify early non-responders who may benefit from change in treatment approach [31].

The feasibility of biological ART based on functional imaging signal change mid-treatment has been shown possible in a single-arm Phase 2 study [32]. Kong *et al.*, used 2-[¹⁸F]-fluoro-2-deoxy-D-glucose positron-emission tomography CT (FDG-PET CT) mid-treatment to inform the volume for dose escalation (up to 80 Gy in 30 fractions) in patients with inoperable stage II–III non-small cell lung cancer [32]. Similarly, DWI signal change during radiotherapy could be used to inform adaptation and dose escalation in relevant tumours [29]. Randomised control studies would be necessary to ensure no adverse impact on disease control occurred, as the shrinking metabolic target might inadvertently reduce coverage of macroscopic or microscopic disease [27].

The challenges of MRI acquisition and planning using an integrated MRI radiotherapy platform have been addressed in the accompanying articles in this special edition.

ART Techniques

Offline ART Solutions

Offline ART aims to correct for the systematic changes to either the target or OARs identified by in-room imaging during the course of treatment. Plan modification, however, takes place offline often adopting the same workflow as the original plan creation including repeat simulation. This is currently the commonest approach to accommodate changes that cannot be corrected by couch shift alone [8,9].

It is most often encountered when changes in patient contour are seen on CBCT because of weight change or treatment response during conventionally fractionated courses. These changes trigger the creation of a new plan in an attempt to improve dosimetry and achieve the planned prescription for the remaining fractions [33]. Until recently, this would have required a similar amount of time as generating the original plan, so limiting the frequency of adaptation but developments in automated contour propagation and automatic plan re-optimisation open the possibility of more frequent plan adjustments [34,35].

When online image guidance informs offline adaptation, authors occasionally refer to this approach as 'hybrid adaptation' [17,36]. Hybrid and offline ART protocols offer the opportunity for patients to benefit from ART enabled by MRI guidance without an integrated MRI radiotherapy system using either a diagnostic MRI scanner, MRI simulator, or a shuttle-based MRI-guided radiotherapy system (MRI on rails) [37,38].

Although no consensus regarding the threshold to trigger offline ART exists, planning studies repeatedly show that a static patient model created at simulation is often obsolete and non-representative of the treatment course. Any adaption, even if implemented at a single time point during a conventionally fractionated treatment course, delivers dosimetric improvement above a single planning scan [33]. Oh *et al.*, showed that weekly online MRI with offline intensity-modulated radiotherapy (IMRT) re-planning using a 3 mm PTV margin in cervical cancer patients accounts for intrafraction pelvic organ motion and tumour shrinkage with measurably improved target coverage when compared to no or a single re-plan [17].

In many tumour types, daily imaging offers an advantage [39–41]. Decreasing the image frequency potentially increases the proportion of fractions associated with significant localisation errors. For example, in prostate cancer radiotherapy, decreasing the imaging frequency from daily to alternate day imaging, results in step up errors of >5 mm in 24% of fractions, which increases to approximately 40% when the set-up error threshold is >3 mm [39].

The logistics of repeated MRI outside the treatment room could be challenging; however, the feasibility for an offline ART protocol, informed by daily out-of-room MRI guidance has been shown to be possible using a shuttle-based MRI workflow in pelvic malignancies [38]. Median total treatment time for each fraction, including time for patient positioning, MRI acquisition, shuttle transfer to treatment suite, patient repositioning, CBCT acquisition, and IMRT delivery was over 1 hour (61 minutes; range 47–99 minutes) [38].

Symptomatic patients are unlikely to tolerate prolonged immobilisation very well. They are also more likely to have larger positional inaccuracies between out-of-room MRI and radiotherapy [38]. The long gap between MRI and treatment also means intrafractional organ motion uncertainties persist [13]. So, although offline/hybrid approaches may help bridge demands for MRI-enabled ART, alternative ART approaches are necessary to address both inter- and intrafraction motion.

Online ART Solutions

Online Adaptive Re-planning

Online adaptive re-planning necessitates a rapid workflow that brings together online imaging, image registration, contour propagation, plan re-optimisation, quality assurance, and treatment delivery all while the patient is on the treatment couch (Figure 2) [42].

Monte Carlo dose calculations are recognised as being the most accurate method for radiotherapy treatment planning, but until recently they had been constrained by long computational times precluding their use for rapid dose calculation. Proposed ways to accelerate Monte Carlo dose calculations are with graphical processing unit (GPU) technology, clusters of central processing units (CPUs), or cloud-based solutions [43–45]. Monte Carlo-based treatment planning systems are also needed to reliably model dose for any integrated MRI radiotherapy platform where the beam passes through the magnetic field. This is necessary because when the magnetic field is orthogonal to the radiation beam, the trajectories of secondary electrons are altered owing to the Lorentz force, resulting in high dose deposition at air-tissue interfaces, and so altering beam profiles than would otherwise be expected [46,47].

In its simplest forms online adaptation involves patient repositioning by shifting the plan to the relative anatomy seen on the day. This can be achieved by a simple couch shift to accommodate the interfraction change with no additional optimisation of the initial treatment plan [48,49]. This strategy provides only first-order correction, as target rotations, volume and shape change, and the geometric relationship to surrounding normal structures are not fully considered [50]. It is arguably more consistent with the definition of IGRT than ART, given that no plan revision takes place as a result of the acquired imaging [27]. An alternative online partial compensation for translational and rotational anatomy change involves adjusting pre-treatment gantry and collimator angles [51,52].

'Plan of the day' solution accesses a library of pre-prepared plans selected for treatment according to best anatomical fit for that fraction [53–56]. Although no further

re-optimisation occurs, target size, position, deformation, and geometric relationship to adjacent structures are considered in part for the library creation [57]. For example, 'plan of the day' for cervical cancer radiotherapy utilises bladder filling to generate a model predicted ITV that is then used to inform the library creation [54].

'Virtual couch shift' or 'dose shift' approach translates and rotates the pre-treatment dose distribution (without new contour regeneration) to compensate for the positional changes in patient's anatomy. An alternative plan is automatically generated and delivered, producing a clinically similar dose distribution to pre-treatment, but at the new position [58]. This dose shift strategy is independent of any couch limitations and is therefore an important solution for the MRI-linear accelerator (linac) (Elekta AB, Stockholm, Sweden), which at present does not allow table shifts [59].

Use of a deformation field has also provided a solution for a number of other online adaptive re-planning strategies [60–62]. The method is essentially reliant on deriving a three-dimensional (3D) geometrical transformational matrix from the planning scan and the image of the day, and using it to 'morph' the treatment plan as an online correction method. An alternative approach is to perform online ART based on a new target outline [50]. A number of single centres have successfully implemented online ART re-planning workflows, demonstrating both feasibility and dosimetric benefit of this approach [42,60,63,64].

Acharya *et al.* utilising the MRIdian platform (ViewRay Inc., Oakwood Village, OH, USA) illustrate clinical feasibility of treating abdominal malignancies with gated motion management and conventional fractionation. An online re-optimisation trigger was based on maintaining pre-determined target and OARs dose–volume histogram (DVH) constraints when the initial plan to anatomy of the day was fused. If the PTV dose was inadequate or the critical structure dose was exceeded, re-optimisation was performed on the anatomy of the day. Using this criterion, 30.6% (52/170) fractions were treated with online re-optimisation and 54.1% (92/170) fractions were treated with either an online adapted plan or previously adapted plan [42].

In a prospective Phase I study, stereotactic MRI-guided online ART was used to treat primary abdominal tumours. Initial plan performance was evaluated on the MRI 'anatomy of the day'. Using this approach, 84% (81/97) fractions were treated with online adaptation. Although the majority of fractions (63%; 61/97) necessitated adaptation because OARs DVH constraints would have been violated if the initial plan had been used, in 21% (20/97) of fractions anatomy of the day appeared favourable for dose escalation while maintaining strict OAR constraints [65].

For primary abdominal malignancies, such as locally advanced pancreatic cancer, the ability to dose escalate has the potential to improve clinical outcomes [66]. Without online MRI informed re-optimisation, radiation dose has been limited to sub-ablative levels because of poor visualisation of OARs and normal tissue toxicity [67].

Simulation studies reflect that daily online adaptation would also provide a dosimetric advantage at other

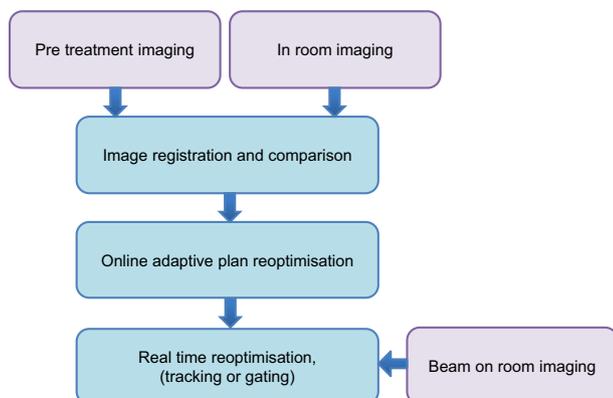


Fig 2. Typical workflow of ART.

anatomical sites. For example, in the pelvis, daily re-optimisation in bladder cancer radiotherapy based on anatomy of the day is superior to both PTV with population derived margins, i.e., no adaptation, and to ‘plan of the day’ approach. This is achieved with a decrease in PTV size and subsequent reduction in normal bowel irradiation [40]. Similarly, in cervical cancer, online re-planning using MRI guidance reduces the absolute volume of small bowel receiving more than 45 Gy (V45Gy) by approximately 100 cm³ [68].

Advanced Motion Management: Gating

Any effective ART strategy is reliant on its ability to acquire high-quality online images with high geometric and temporal resolution [69,70]. The greater the delay between imaging and treatment, the greater the opportunities for short-term organ motion [13]. Integrated MRI-guided platforms enable rapid high-quality imaging to take place immediately before and during the delivery of each radiotherapy fraction. This ‘beam-on’ imaging means motion monitoring occurs during treatment delivery and is able to provide opportunity for ‘real-time’ anatomical feedback to inform adaptation. Motion blurring is reduced by speed of MRI data acquisition.

Intrafractional motion varies according to tumour position within the body [71,72]. Breathing motion can result in target lesions in the lung or intra-abdominal cavity moving several millimetres or several centimetres [73,74]. To try and capture tumour motion throughout the breathing cycle, four-dimensional (4D) CT has been used to inform a personalised internal target volume (ITV). Breathing motion, however, is often unpredictable, and single 4D CT is rarely representative of true range of motion through treatment and so requires application of large treatment margins to avoid geographical miss [75–77].

Gating mitigates intrafractional motion by delivering dose only when target is within a defined geographical position. By convention, position recognition for gating has been reliant on either being able to see the target on CBCT, the use of external surrogates [78], implanted radiopaque markers [79] or electromagnetic transponders [80]. These methods successfully improve geometric and dosimetric accuracy compared to non-gated approaches [81].

An MRI-gated solution provides adequate visualisation of the target and therefore can be performed without implanted devices or potentially unreliable external surrogates [82]. Gating without implanted devices or external surrogates is currently in use within the MRIdian system (ViewRay Inc.). Using this approach the GTV to PTV margin has been reduced from 5 to 2 mm for stereotactic ablative radiotherapy [63].

Advanced Motion Management: Tracking

Tracking is a technique whereby the target is ‘followed’ by the radiation beam, and treatment delivery parameters are continually adjusted to compensate for tumour motion. The target remains within the beams eye view at all times.

Unlike gating, the treatment machine is always on and so treatment times are expected to be comparably shorter [83].

Tracking can be achieved in one of three ways: it is possible to shift the treatment source to track tumour motion, to shift the beam using multi-leaf collimators (MLCs), or adjust the patient position relative to the stationary beam [84]. Robotic, gimbaled, MLC, and couch-tracking systems are all solutions implemented for tumour tracking [84–86]. They rely on CT and kilovoltage image guidance or implanted devices.

MRI-guided tracking is possible because the superior soft-tissue definition allows easy identification of target and OARs deformation and rotation [87]. This is advantageous because surrogates for tumour position have limitations in their ability to accurately describe motion [88–90].

In a proof of concept study, it has been possible to track motion using MLCs in combination with a fast one-dimensional (1D) MRI sequence [83]. An MRI-guided two-dimensional (2D) tracking solution has also been determined [90]. Although MRI-informed tracking is not yet in clinical practice, it is expected to be possible soon. Simulation work in lung cancer cases suggests when clinically implemented, it would be expected to spare healthy tissue, including reducing the mean lung, skin, and great vessels dose while maintaining dose to 98% of GTV compared to conventional dose deliveries [91]. The reported improvements in normal tissue irradiation reflect ability to deliver treatment using tracking on a gantry-based linac with reduced PTV size compared to the standard ITV approach. If this technique were to be applied for the treatment of lung and pancreatic cancer, the PTV could be reduced by up to 40% and 17%, respectively [92,93].

Real-Time Adaptive Re-planning

Real-time ART has the potential to improve accuracy of the delivered dose to target with normal tissue sparing, independent of the delivery system [84]. This suggests that each fraction should be adapted irrespective of pre-determined action levels. Adapting the plan during beam delivery necessitates continuous imaging with a real-time motion management method, re-planning, and rapid dose calculation.

The team from the University Medical Centre Utrecht recently published a potential solution to this problem illustrated in a proof of principle study based on their Elekta MR-linac (Elekta AB, Stockholm, Sweden). This study describes a novel real-time adaptive treatment pathway where intrafraction, inter-beam re-planning and optimisation takes place, taking into account the previously delivered dose within that fraction accumulated onto the underlying moving anatomy [94].

Fast inverse IMRT re-planning based on the updated 3D anatomy during intrafraction delivery was possible in part because of a treatment planning method called adaptive sequencer (ASEQ) [95]. ASEQ is an iterative process that begins with initial optimisation that faithfully reflects the ideal/prescribed dose. Each iteration produces unique

segments that follow the anatomy seen. The dose of that segment is calculated and is subtracted from the ideal dose distribution. The updated dose distribution then informs the next iteration. This is repeated until dose convergence between the delivered and prescribed dose occurs [95,96].

In the context of a single fraction (25 Gy) stereotactic body radiotherapy (SBRT) planning study, application of ASEQ showed that inter-beam IMRT re-planning to a no-margin PTV had theoretical benefit with higher dose target coverage, tighter dose distributions, and improved normal tissue sparing compared to a mid-respiratory position SBRT plan with a 3 mm PTV margin. The high dose region (defined as 2 cm around the target) was decreased by an average of 27.8% with real-time planning [94]. A no-margin PTV was only feasible because MRI data were continuously informing the 3D anatomical deformations of the target and OARs during treatment delivery [94].

Future Considerations for MRI-Guided ART

It is attractive to envision that we are entering a new era of radiotherapy. MRI-guided ART enabled by technological and computational advances has increased the precision of RT with potential increase in the therapeutic window. We would, however, advocate caution, as we are yet to demonstrate that the dosimetric gains seen will translate to meaningful clinical outcomes for our patients [97].

It is certain that not all patients will derive the same benefit with ART. Prospective evaluation within a robust framework is necessary [98,99]. Well-designed clinical trials remain the optimal method to evaluate patient benefit of this technology; however, head-to-head comparative studies of CT-guided and MRI-guided ART using standard dose and fractionations delivered to an anatomical target may not be ambitious enough to demonstrate the true potential of MRI-guided technology in terms of improved toxicity, local control, and survival. Many groups are investigating how MRI-guided ART provides a platform to deliver radiation in circumstances that would have otherwise been impossible. These include ultrahypofractionation (single radical fraction) in regions of organ motion [100], safer re-irradiation [101], and integrating on-board functional MRI sequences to inform biological feedback for personalised adaptation [102]. The future of ART will be MRI guided, but how we choose to best apply this tool in order for it to be measurably transformative for patient outcomes remains to be determined.

Acknowledgements

We acknowledge NHS funding to the NIHR Biomedical Research Centre for Cancer and to Cancer Research UK (programme grant C33589/A19727). The Royal Marsden Hospital and The Institute of Cancer Research are members of the Elekta MR-linac Consortium, which aims to coordinate international collaborative research relating to the Elekta Unity (MR-linac). Elekta (Elekta AB, Stockholm, Sweden) and Philips (Philips, Best, Netherlands) are

commercial members of the MR-linac Consortium. Elekta financially supports consortium member institutions with research funding and travel costs for consortium meetings. A.H., V.H., U.O., S.N., and S.H. have received educational, research, and, or travel support from Elekta within this context. No commercial financial support was received from any organisation for the submitted work.

Appendix A. Supplementary data

Supplementary data related to this article can be found at <https://doi.org/10.1016/j.clon.2018.08.001>.

References

- [1] International Committee on Radiation Units and Measurements. *ICRU report 83 prescribing, recording, and reporting intensity-modulated photon-beam therapy*. IMRT); 2010.
- [2] International Committee on Radiation Units and Measurements. *ICRU report 62, prescribing, recording and reporting photon beam therapy* 1999. Supplement to ICRU Report 50.
- [3] van Herk M, Remeijer P, Lebesque JV. Inclusion of geometric uncertainties in treatment plan evaluation. *Int J Radiat Oncol Biol Phys* 2002;52(5):1407–1422.
- [4] Dearnaley DP, Jovic G, Syndikus I, Khoo V, Cowan RA, Graham JD, et al. Escalated-dose versus control-dose conformal radiotherapy for prostate cancer: long-term results from the MRC RT01 randomised controlled trial. *Lancet Oncol* 2014;15(4):464–473.
- [5] Peeters ST, Heemsbergen WD, Koper PC, van Putten WL, Slot A, Dielwart MF, et al. Dose–response in radiotherapy for localized prostate cancer: results of the Dutch multicenter randomized phase III trial comparing 68 Gy of radiotherapy with 78 Gy. *J Clin Oncol* 2006;24(13):1990–1996.
- [6] Foroudi F, Pham D, Bressel M, Hardcastle N, Gill S, Kron T. Comparison of margins, integral dose and interfraction target coverage with image-guided radiotherapy compared with non-image-guided radiotherapy for bladder cancer. *Clin Oncol (R Coll Radiol)* 2014;26(8):497–505.
- [7] Yan D, Vicini F, Wong J, Martinez A. Adaptive radiation therapy. *Phys Med Biol* 1997;42(1):123–132.
- [8] Yan D, Wong J, Vicini F, Michalski J, Pan C, Frazier A, et al. Adaptive modification of treatment planning to minimize the deleterious effects of treatment setup errors. *Int J Radiat Oncol Biol Phys* 1997;38(1):197–206.
- [9] Yan D, Lockman D, Brabbins D, Tyburski L, Martinez A. An offline strategy for constructing a patient-specific planning target volume in adaptive treatment process for prostate cancer. *Int J Radiat Oncol Biol Phys* 2000;48(1):289–302.
- [10] Njeh CF. Tumor delineation: the weakest link in the search for accuracy in radiotherapy. *J Med Phys* 2008;33(4):136–140.
- [11] Roques TW. Patient selection and radiotherapy volume definition — can we improve the weakest links in the treatment chain? *Clin Oncol (R Coll Radiol)* 2014;26(6):353–355.
- [12] Weiss E, Hess CF. The impact of gross tumor volume (GTV) and clinical target volume (CTV) definition on the total accuracy in radiotherapy theoretical aspects and practical experiences. *Strahlenther Onkol* 2003;179(1):21–30.
- [13] van Herk M. Errors and margins in radiotherapy. *Semin Radiat Oncol* 2004;14(1):52–64.

- [14] Saarnak AE, Boersma M, van Bunningen BN, Wolterink R, Steggerda MJ. Inter-observer variation in delineation of bladder and rectum contours for brachytherapy of cervical cancer. *Radiother Oncol* 2000;56(1):37–42.
- [15] Noel CE, Parikh PJ, Spencer CR, Green OL, Hu Y, Mutic S, et al. Comparison of onboard low-field magnetic resonance imaging versus onboard computed tomography for anatomy visualization in radiotherapy. *Acta Oncol* 2015;54(9):1474–1482.
- [16] Lutgendorf-Caucig C, Fotina I, Stock M, Potter R, Goldner G, Georg D. Feasibility of CBCT-based target and normal structure delineation in prostate cancer radiotherapy: multi-observer and image multi-modality study. *Radiother Oncol* 2011;98(2):154–161.
- [17] Oh S, Stewart J, Moseley J, Kelly V, Lim K, Xie J, et al. Hybrid adaptive radiotherapy with online MRI in cervix cancer IMRT. *Radiother Oncol* 2014;110(2):323–328.
- [18] Dubois DF, Prestidge BR, Hotchkiss LA, Prete JJ, Bice Jr WS. Intraobserver and interobserver variability of MR imaging- and CT-derived prostate volumes after transperineal interstitial permanent prostate brachytherapy. *Radiology* 1998;207(3):785–789.
- [19] Rasch C, Barillot I, Remeijer P, Touw A, van Herk M, Lebesque JV. Definition of the prostate in CT and MRI: a multi-observer study. *Int J Radiat Oncol Biol Phys* 1999;43(1):57–66.
- [20] Ahmed M, Schmidt M, Sohaib A, Kong C, Burke K, Richardson C, et al. The value of magnetic resonance imaging in target volume delineation of base of tongue tumours—a study using flexible surface coils. *Radiother Oncol* 2010;94(2):161–167.
- [21] Tao CJ, Yi JL, Chen NY, Ren W, Cheng J, Tung S, et al. Multi-subject atlas-based auto-segmentation reduces interobserver variation and improves dosimetric parameter consistency for organs at risk in nasopharyngeal carcinoma: a multi-institution clinical study. *Radiother Oncol* 2015;115(3):407–411.
- [22] O'Neill BD, Salerno G, Thomas K, Tait DM, Brown G. MR vs CT imaging: low rectal cancer tumour delineation for three-dimensional conformal radiotherapy. *Br J Radiol* 2009;82(978):509–513.
- [23] Rasch C, Keus R, Pameijer FA, Koops W, de Ru V, Muller S, et al. The potential impact of CT-MRI matching on tumor volume delineation in advanced head and neck cancer. *Int J Radiat Oncol Biol Phys* 1997;39(4):841–848.
- [24] Steenbakkers RJ, Deurloo KE, Nowak PJ, Lebesque JV, van Herk M, Rasch CR. Reduction of dose delivered to the rectum and bulb of the penis using MRI delineation for radiotherapy of the prostate. *Int J Radiat Oncol Biol Phys* 2003;57(5):1269–1279.
- [25] Potter R, Dimopoulos J, Georg P, Lang S, Waldhausl C, Wachter-Gerstner N, et al. Clinical impact of MRI assisted dose volume adaptation and dose escalation in brachytherapy of locally advanced cervix cancer. *Radiother Oncol* 2007;83(2):148–155.
- [26] Chen AM, Farwell DG, Luu Q, Chen LM, Vijayakumar S, Purdy JA. Marginal misses after postoperative intensity-modulated radiotherapy for head and neck cancer. *Int J Radiat Oncol Biol Phys* 2011;80(5):1423–1429.
- [27] Verellen D, De Ridder M, Linthout N, Tournel K, Soete G, Storme G. Innovations in image-guided radiotherapy. *Nat Rev Cancer* 2007;7(12):949–960.
- [28] Meng J, Zhu L, Zhu L, Xie L, Wang H, Liu S, et al. Whole-lesion ADC histogram and texture analysis in predicting recurrence of cervical cancer treated with CCRT. *Oncotarget* 2017;8(54):92442–92453.
- [29] Wong KH, Panek R, Dunlop A, McQuaid D, Riddell A, Welsh LC, et al. Changes in multimodality functional imaging parameters early during chemoradiation predict treatment response in patients with locally advanced head and neck cancer. *Eur J Nucl Med Mol Imaging* 2018;45(5):759–767.
- [30] Barbaro B, Vitale R, Valentini V, Illuminati S, Vecchio FM, Rizzo G, et al. Diffusion-weighted magnetic resonance imaging in monitoring rectal cancer response to neoadjuvant chemoradiotherapy. *Int J Radiat Oncol Biol Phys* 2012;83(2):594–599.
- [31] Hafeez S, Huddart R. Advances in bladder cancer imaging. *BMC Med* 2013;11:104.
- [32] Kong FM, Ten Haken RK, Schipper M, Frey KA, Hayman J, Gross M, et al. Effect of midtreatment PET/CT-adapted radiation therapy with concurrent chemotherapy in patients with locally advanced non-small-cell lung cancer: a Phase 2 clinical trial. *JAMA oncol* 2017;3(10):1358–1365.
- [33] Schwartz DL, Garden AS, Shah SJ, Chronowski G, Sejjal S, Rosenthal DI, et al. Adaptive radiotherapy for head and neck cancer—dosimetric results from a prospective clinical trial. *Radiother Oncol* 2013;106(1):80–84.
- [34] Heijmen B, Voet P, Franssen D, Penninkhof J, Milder M, Akhlat H, et al. Fully automated, multi-criterial planning for volumetric modulated arc therapy — an international multi-center validation for prostate cancer. *Radiother Oncol* 2018;128(2):343–348.
- [35] Li N, Zarepisheh M, Uribe-Sanchez A, Moore K, Tian Z, Zhen X, et al. Automatic treatment plan re-optimization for adaptive radiotherapy guided with the initial plan DVHs. *Phys Med Biol* 2013;58(24):8725–8738.
- [36] Lei Y, Wu Q. A hybrid strategy of offline adaptive planning and online image guidance for prostate cancer radiotherapy. *Phys Med Biol* 2010;55(8):2221–2234.
- [37] Jaffray DA, Carlone MC, Milosevic MF, Breen SL, Stanescu T, Rink A, et al. A facility for magnetic resonance-guided radiation therapy. *Semin Radiat Oncol* 2014;24(3):193–195.
- [38] Bostel T, Pfaffenberger A, Delorme S, Dreher C, Echner G, Haering P, et al. Prospective feasibility analysis of a novel offline approach for MR-guided radiotherapy. *Strahlenther Onkol* 2018;194(5):425–434.
- [39] Kupelian PA, Lee C, Langen KM, Zeidan OA, Manon RR, Willoughby TR, et al. Evaluation of image-guidance strategies in the treatment of localized prostate cancer. *Int J Radiat Oncol Biol Phys* 2008;70(4):1151–1157.
- [40] Vestergaard A, Hafeez S, Muren LP, Nill S, Hoyer M, Hansen VN, et al. The potential of MRI-guided online adaptive re-optimisation in radiotherapy of urinary bladder cancer. *Radiother Oncol* 2016;118(1):154–159.
- [41] Henke L, Kashani R, Yang D, Zhao T, Green O, Olsen L, et al. Simulated online adaptive magnetic resonance-guided stereotactic body radiation therapy for the treatment of oligometastatic disease of the abdomen and central thorax: characterization of potential advantages. *Int J Radiat Oncol Biol Phys* 2016;96(5):1078–1086.
- [42] Acharya S, Fischer-Valuck BW, Kashani R, Parikh P, Yang D, Zhao T, et al. Online magnetic resonance image guided adaptive radiation therapy: first clinical applications. *Int J Radiat Oncol Biol Phys* 2016;94(2):394–403.
- [43] Jia X, George Xu X, Orton CG. Point/counterpoint. GPU technology is the hope for near real-time Monte Carlo dose calculations. *Med Phys* 2015;42(4):1474–1476.

- [44] Ziegenhein P, Kozin IN, Kamerling CP, Oelfke U. Towards real-time photon Monte Carlo dose calculation in the cloud. *Phys Med Biol* 2017;62(11):4375–4389.
- [45] Men C, Gu X, Choi D, Majumdar A, Zheng Z, Mueller K, et al. GPU-based ultrafast IMRT plan optimization. *Phys Med Biol* 2009;54(21):6565–6573.
- [46] Raaijmakers AJ, Raaymakers BW, Lagendijk JJ. Integrating a MRI scanner with a 6 MV radiotherapy accelerator: dose increase at tissue–air interfaces in a lateral magnetic field due to returning electrons. *Phys Med Biol* 2005;50(7):1363–1376.
- [47] Raaymakers BW, Raaijmakers AJ, Kotte AN, Jette D, Lagendijk JJ. Integrating a MRI scanner with a 6 MV radiotherapy accelerator: dose deposition in a transverse magnetic field. *Phys Med Biol* 2004;49(17):4109–4118.
- [48] Ghilezan M, Yan D, Liang J, Jaffray D, Wong J, Martinez A. Online image-guided intensity-modulated radiotherapy for prostate cancer: how much improvement can we expect? A theoretical assessment of clinical benefits and potential dose escalation by improving precision and accuracy of radiation delivery. *Int J Radiat Oncol Biol Phys* 2004;60(5):1602–1610.
- [49] Letourneau D, Martinez AA, Lockman D, Yan D, Vargas C, Ivaldi G, et al. Assessment of residual error for online cone-beam CT-guided treatment of prostate cancer patients. *Int J Radiat Oncol Biol Phys* 2005;62(4):1239–1246.
- [50] Ahunbay EE, Peng C, Chen GP, Narayanan S, Yu C, Lawton C, et al. An online re-planning scheme for interfractional variations. *Med Phys* 2008;35(8):3607–3615.
- [51] Rijkhorst EJ, Lakeman A, Nijkamp J, de Bois J, van Herk M, Lebesque JV, et al. Strategies for online organ motion correction for intensity-modulated radiotherapy of prostate cancer: prostate, rectum, and bladder dose effects. *Int J Radiat Oncol Biol Phys* 2009;75(4):1254–1260.
- [52] Mohan R, Zhang X, Wang H, Kang Y, Wang X, Liu H, et al. Use of deformed intensity distributions for online modification of image-guided IMRT to account for interfractional anatomic changes. *Int J Radiat Oncol Biol Phys* 2005;61(4):1258–1266.
- [53] Hafeez S, McDonald F, Lalondrelle S, McNair H, Warren-Oseni K, Jones K, et al. Clinical outcomes of image guided adaptive hypofractionated weekly radiation therapy for bladder cancer in patients unsuitable for radical treatment. *Int J Radiat Oncol Biol Phys* 2017;98(1):115–122.
- [54] Heijkoop ST, Langerak TR, Quint S, Bondar L, Mens JW, Heijmen BJ, et al. Clinical implementation of an online adaptive plan-of-the-day protocol for nonrigid motion management in locally advanced cervical cancer IMRT. *Int J Radiat Oncol Biol Phys* 2014;90(3):673–679.
- [55] Xia P, Qi P, Hwang A, Kinsey E, Pouliot J, Roach 3rd M. Comparison of three strategies in management of independent movement of the prostate and pelvic lymph nodes. *Med Phys* 2010;37(9):5006–5013.
- [56] Lutkenhaus LJ, de Jong R, Geijssen ED, Visser J, van Wieringen N, Bel A. Potential dosimetric benefit of an adaptive plan selection strategy for short-course radiotherapy in rectal cancer patients. *Radiother Oncol* 2016;119(3):525–530.
- [57] Bondar ML, Hoogeman MS, Mens JW, Quint S, Ahmad R, Dhawtal G, et al. Individualized nonadaptive and online-adaptive intensity-modulated radiotherapy treatment strategies for cervical cancer patients based on pretreatment acquired variable bladder filling computed tomography scans. *Int J Radiat Oncol Biol Phys* 2012;83(5):1617–1623.
- [58] Bol GH, Lagendijk JJ, Raaymakers BW. Virtual couch shift (VCS): accounting for patient translation and rotation by online IMRT re-optimization. *Phys Med Biol* 2013;58(9):2989–3000.
- [59] Raaymakers BW, Lagendijk JJ, Overweg J, Kok JG, Raaijmakers AJ, Kerkhof EM, et al. Integrating a 1.5 T MRI scanner with a 6 MV accelerator: proof of concept. *Phys Med Biol* 2009;54(12):N229–N237.
- [60] Bohoudi O, Bruynzeel AME, Senan S, Cuijpers JP, Slotman BJ, Lagerwaard FJ, et al. Fast and robust online adaptive planning in stereotactic MR-guided adaptive radiation therapy (SMART) for pancreatic cancer. *Radiother Oncol* 2017;125(3):439–444.
- [61] Ahunbay EE, Li XA. Gradient maintenance: a new algorithm for fast online re-planning. *Med Phys* 2015;42(6):2863–2876.
- [62] Feng Y, Castro-Pareja C, Shekhar R, Yu C. Direct aperture deformation: an interfraction image guidance strategy. *Med Phys* 2006;33(12):4490–4498.
- [63] Fischer-Valuck BW, Henke L, Green O, Kashani R, Acharya S, Bradley JD, et al. Two-and-a-half-year clinical experience with the world's first magnetic resonance image guided radiation therapy system. *Adv Radiat Oncol* 2017;2(3):485–493.
- [64] Raaymakers BW, Jurgenliemk-Schulz IM, Bol GH, Glitzner M, Kotte A, van Asselen B, et al. First patients treated with a 1.5 T MRI-Linac: clinical proof of concept of a high-precision, high-field MRI guided radiotherapy treatment. *Phys Med Biol* 2017;62(23):L41–L50.
- [65] Henke L, Kashani R, Robinson C, Curcuru A, DeWees T, Bradley J, et al. Phase I trial of stereotactic MR-guided online adaptive radiation therapy (SMART) for the treatment of oligometastatic or unresectable primary malignancies of the abdomen. *Radiother Oncol* 2018;126(3):519–526.
- [66] Krishnan S, Chadha AS, Suh Y, Chen HC, Rao A, Das P, et al. Focal radiation therapy dose escalation improves overall survival in locally advanced pancreatic cancer patients receiving induction chemotherapy and consolidative chemoradiation. *Int J Radiat Oncol Biol Phys* 2016;94(4):755–765.
- [67] Crane CH. Hypofractionated ablative radiotherapy for locally advanced pancreatic cancer. *J Radiat Res* 2016;57(Suppl. 1):i53–i57.
- [68] Kerkhof EM, Raaymakers BW, van der Heide UA, van de Bunt L, Jurgenliemk-Schulz IM, Lagendijk JJ. Online MRI guidance for healthy tissue sparing in patients with cervical cancer: an IMRT planning study. *Radiother Oncol* 2008;88(2):241–249.
- [69] Crijs SP, Bakker CJ, Seevinck PR, de Leeuw H, Lagendijk JJ, Raaymakers BW. Towards inherently distortion-free MR images for image-guided radiotherapy on an MRI accelerator. *Phys Med Biol* 2012;57(5):1349–1358.
- [70] Huang KC, Cao Y, Baharom U, Balter JM. Phantom-based characterization of distortion on a magnetic resonance imaging simulator for radiation oncology. *Phys Med Biol* 2016;61(2):774–790.
- [71] Ghilezan MJ, Jaffray DA, Siewerdsen JH, Van Herk M, Shetty A, Sharpe MB, et al. Prostate gland motion assessed with cine-magnetic resonance imaging (cine-MRI). *Int J Radiat Oncol Biol Phys* 2005;62(2):406–417.
- [72] McPartlin AJ, Li XA, Kershaw LE, Heide U, Kerkmeijer L, Lawton C, et al. MRI-guided prostate adaptive radiotherapy — a systematic review. *Radiother Oncol* 2016;119(3):371–380.
- [73] Seppenwoolde Y, Shirato H, Kitamura K, Shimizu S, van Herk M, Lebesque JV, et al. Precise and real-time measurement of 3D tumor motion in lung due to breathing and

- heartbeat, measured during radiotherapy. *Int J Radiat Oncol Biol Phys* 2002;53(4):822–834.
- [74] Heerkens HD, van Vulpen M, van den Berg CA, Tijssen RH, Crijns SP, Molenaar IQ, et al. MRI-based tumor motion characterization and gating schemes for radiation therapy of pancreatic cancer. *Radiother Oncol* 2014;111(2):252–257.
- [75] James SS, Mishra P, Hacker F, Berbeco RI, Lewis JH. Quantifying ITV instabilities arising from 4DCT: a simulation study using patient data. *Phys Med Biol* 2012;57(5):L1–L7.
- [76] Ge J, Santanam L, Noel C, Parikh PJ. Planning 4-dimensional computed tomography (4DCT) cannot adequately represent daily intrafractional motion of abdominal tumors. *Int J Radiat Oncol Biol Phys* 2013;85(4):999–1005.
- [77] Keall PJ, Mageras GS, Balter JM, Emery RS, Forster KM, Jiang SB, et al. The management of respiratory motion in radiation oncology report of AAPM Task Group 76. *Med Phys* 2006;33(10):3874–3900.
- [78] Cole AJ, Hanna GG, Jain S, O'Sullivan JM. Motion management for radical radiotherapy in non-small cell lung cancer. *Clin Oncol (R Coll Radiol)* 2014;26(2):67–80.
- [79] Shimizu S, Nishioka K, Suzuki R, Shinohara N, Maruyama S, Abe T, et al. Early results of urethral dose reduction and small safety margin in intensity-modulated radiation therapy (IMRT) for localized prostate cancer using a real-time tumor-tracking radiotherapy (RTRT) system. *Radiat Oncol* 2014;9:118.
- [80] Kupelian P, Willoughby T, Mahadevan A, Djemil T, Weinstein G, Jani S, et al. Multi-institutional clinical experience with the Calypso System in localization and continuous, real-time monitoring of the prostate gland during external radiotherapy. *Int J Radiat Oncol Biol Phys* 2007;67(4):1088–1098.
- [81] Worm ES, Hoyer M, Hansen R, Larsen LP, Weber B, Grau C, et al. A prospective cohort study of gated stereotactic liver radiation therapy using continuous internal electromagnetic motion monitoring. *Int J Radiat Oncol Biol Phys* 2018;101(2):366–375.
- [82] Hoisak JD, Sixel KE, Tirona R, Cheung PC, Pignol JP. Correlation of lung tumor motion with external surrogate indicators of respiration. *Int J Radiat Oncol Biol Phys* 2004;60(4):1298–1306.
- [83] Crijns SP, Raaymakers BW, Lagendijk JJ. Proof of concept of MRI-guided tracked radiation delivery: tracking one-dimensional motion. *Phys Med Biol* 2012;57(23):7863–7872.
- [84] Colvill E, Booth J, Nill S, Fast M, Bedford J, Oelfke U, et al. A dosimetric comparison of real-time adaptive and non-adaptive radiotherapy: a multi-institutional study encompassing robotic, gimbaled, multileaf collimator and couch tracking. *Radiother Oncol* 2016;119(1):159–165.
- [85] Keall PJ, Nguyen DT, O'Brien R, Caillet V, Hewson E, Poulsen PR, et al. The first clinical implementation of real-time image-guided adaptive radiotherapy using a standard linear accelerator. *Radiother Oncol* 2018;127(1):6–11.
- [86] Lang S, Zeimet J, Ochsner G, Schmid Daners M, Riesterer O, Klock S. Development and evaluation of a prototype tracking system using the treatment couch. *Med Phys* 2014;41(2):021720.
- [87] Fast MF, Kamerling CP, Ziegenhein P, Menten MJ, Bedford JL, Nill S, et al. Assessment of MLC tracking performance during hypofractionated prostate radiotherapy using real-time dose reconstruction. *Phys Med Biol* 2016;61(4):1546–1562.
- [88] Malinowski K, McAvoy TJ, George R, Dietrich S, D'Souza WD. Incidence of changes in respiration-induced tumor motion and its relationship with respiratory surrogates during individual treatment fractions. *Int J Radiat Oncol Biol Phys* 2012;82(5):1665–1673.
- [89] van der Horst A, Lens E, Wognum S, de Jong R, van Hooft JE, van Tienhoven G, et al. Limited role for biliary stent as surrogate fiducial marker in pancreatic cancer: stent and intratumoral fiducials compared. *Int J Radiat Oncol Biol Phys* 2014;89(3):641–648.
- [90] Yun J, Wachowicz K, Mackenzie M, Rathee S, Robinson D, Fallone BG. First demonstration of intrafractional tumor-tracked irradiation using 2D phantom MR images on a prototype linac-MR. *Med Phys* 2013;40(5):051718.
- [91] Menten MJ, Fast MF, Nill S, Kamerling CP, McDonald F, Oelfke U. Lung stereotactic body radiotherapy with an MR-linac — quantifying the impact of the magnetic field and real-time tumor tracking. *Radiother Oncol* 2016;119(3):461–466.
- [92] Ehrbar S, Johl A, Tartas A, Stark LS, Riesterer O, Klock S, et al. ITV, mid-ventilation, gating or couch tracking — a comparison of respiratory motion-management techniques based on 4D dose calculations. *Radiother Oncol* 2017;124(1):80–88.
- [93] Karava K, Ehrbar S, Riesterer O, Roesch J, Glatz S, Klock S, et al. Potential dosimetric benefits of adaptive tumor tracking over the internal target volume concept for stereotactic body radiation therapy of pancreatic cancer. *Radiat Oncol* 2017;12(1):175.
- [94] Kontaxis C, Bol GH, Stemkens B, Glitzner M, Prins FM, Kerkmeijer LGW, et al. Towards fast online intrafraction replanning for free-breathing stereotactic body radiation therapy with the MR-linac. *Phys Med Biol* 2017;62(18):7233–7248.
- [95] Kontaxis C, Bol GH, Lagendijk JJ, Raaymakers BW. Towards adaptive IMRT sequencing for the MR-linac. *Phys Med Biol* 2015;60(6):2493–2509.
- [96] Kontaxis C, Bol GH, Lagendijk JJ, Raaymakers BW. A new methodology for inter- and intrafraction plan adaptation for the MR-linac. *Phys Med Biol* 2015;60(19):7485–7497.
- [97] van Herk M, McWilliam A, Dubec M, Faivre-Finn C, Choudhury A. Magnetic resonance imaging-guided radiation therapy: a short strengths, weaknesses, opportunities, and threats analysis. *Int J Radiat Oncol Biol Phys* 2018;101(5):1057–1060.
- [98] Verkooijen HM, Kerkmeijer LGW, Fuller CD, Huddart R, Faivre-Finn C, Verheij M, et al. R-IDEAL: a framework for systematic clinical evaluation of technical innovations in radiation oncology. *Front Oncol* 2017;7:59.
- [99] Harrington K, Hall E, Hawkins M, Henry A, MacKay R, Maughan T, et al. Introducing the Cancer Research UK Advanced Radiotherapy Technologies Network (ART-NET). *Clin Oncol (R Coll Radiol)* 2017;29(11):707–710.
- [100] Pathmanathan AU, van As NJ, Kerkmeijer LGW, Christodouleas J, Lawton CAF, Vesprini D, et al. Magnetic resonance imaging-guided adaptive radiation therapy: a “game changer” for prostate treatment? *Int J Radiat Oncol Biol Phys* 2018;100(2):361–373.
- [101] Levin-Epstein R, Cao M, Lee P, Steinberg ML, Lamb J, Raldow AC. Magnetic resonance-guided inter-fraction monitoring opens doors to delivering safer reirradiation: an illustrative case report and discussion. *Cureus* 2018;10(4):e2479.
- [102] Dinapoli N, Barbaro B, Gatta R, Chiloiro G, Casa C, Masciocchi C, et al. Magnetic resonance, vendor-independent, intensity histogram analysis predicting pathologic complete response after radiochemotherapy of rectal cancer. *Int J Radiat Oncol Biol Phys* 2018.