

EANM enabling guide: How to improve the Accessibility of

Clinical Dosimetry

Jonathan Gear¹, Caroline Stokke², Christelle Terwinghe³, Silvano Gnesin⁴, Mattias Sandström⁵, Johannes Tran-Gia⁶, Marta Cremonesi⁷, Francesco Cicone⁸, Fredrik Verburg⁹, Roland Hustinx¹⁰, Luca Giovanella¹¹, Ken Herrmann¹², Pablo Minguez Gabiña¹³.

1) Joint Department of Physics, Royal Marsden NHSFT & Institute of Cancer Research, Sutton, UK

2) Division of Radiology and Nuclear Medicine, Oslo University Hospital, Oslo, Norway & Department of Physics, University of Oslo, Oslo, Norway

3) Department of Nuclear Medicine, Universitair Ziekenhuis Leuven, Leuven, Belgium

4) Institute of Radiation Physics, Lausanne University Hospital, University of Lausanne, Lausanne, Switzerland

5) Section of Nuclear Medicine and PET, Department of Surgical Sciences, Uppsala University, Uppsala, Sweden & Section of Medical Physics, Department of Immunology, Genetics and Pathology, Uppsala University, 751 85, Uppsala

6) Department of Nuclear Medicine, University Hospital Würzburg, Oberdürrbacher Str. 6, 97080 Würzburg, Germany

7) Radiation Research Unit, Department of Medical Imaging and Radiation Sciences, Istituto Europeo di Oncologia, IRCCS, Milan, Italy

8) Department of Experimental and Clinical Medicine, Neuroscience Research Centre, PET/RM Unit, "Magna Graecia" University of Catanzaro, Catanzaro, Italy & Nuclear Medicine Unit, University Hospital "Mater Domini, Catanzaro, Italy

9) Department of Radiology and Nuclear Medicine, Erasmus Medical Center, Rotterdam, the Netherlands

- 26 10) Division of Nuclear Medicine and Oncological Imaging, University Hospital of Liège, Liège,
27 Belgium & GIGA-CRC in vivo imaging, University of Liège, Liège, Belgium
- 28 11) Clinic for Nuclear Medicine and Molecular Imaging, Imaging Institute of Southern Switzerland,
29 Ente Ospedaliero Cantonale, Bellinzona, Switzerland
- 30 12) Department of Nuclear Medicine, University of Duisburg-Essen, Duisburg, Germany &
31 German Cancer Consortium (DKTK)-University Hospital Essen, Essen, Germany
- 32 13) Department of Medical Physics and Radiation Protection, Gurutzeta-Cruces University
33 Hospital/Biocruces Health Research Institute, Barakaldo, Spain & Department of Applied
34 Physics, Faculty of Engineering, UPV/EHU, Bilbao, Spain
- 35 Corresponding Author Contact: jonathan.gear@icr.ac.uk

36 Abstract

37 Dosimetry can be a useful tool for personalization of molecular radiotherapy (MRT)
38 procedures, enabling the continuous development of theranostic concepts. However,
39 the additional resource requirements are often seen as a barrier to implementation.
40 This guide discusses the requirements for dosimetry and demonstrates how a
41 dosimetry regimen can be tailored to the available facilities of a centre. The aim is to
42 help centres wishing to initiate a dosimetry service but may not have the experience
43 or resources of some of the more established therapy and dosimetry centres. The
44 multidisciplinary approach and different personnel requirements are discussed and
45 key equipment reviewed. Example protocols demonstrating these factors are given in
46 the supplementary material for the main therapies carried out in nuclear medicine,
47 including [¹³¹I]-Nal for benign thyroid disorders, [¹⁷⁷Lu]-DOTATATE and ¹³¹I-mIBG for
48 neuroendocrine tumours and [⁹⁰Y]-microspheres for unresectable hepatic carcinoma.

49 Introduction

50 Since the early introductions of radiopharmaceuticals for therapy, there has been
51 continued interest in optimisation and personalisation, to determine the ideal treatment
52 activities and regimens. Of the optimisation strategies developed, dosimetry
53 approaches, such as those adopted by external beam radiation therapy (EBRT) or
54 brachytherapy, arguably have the strongest scientific grounding with the treatment
55 mechanism shown to be that of radiation induced cell kill.

56 In molecular radiotherapy (MRT), some treatment planning procedures have been
57 reported in specific applications [1-5] and dose-effect relationships in several therapy
58 procedures have been highlighted [6-8]. Studies have also exposed the relevant
59 improvements reached by dosimetry-based approaches in terms of progression free

60 survival and overall survival [7-13]. Thus, from a clinical perspective, dosimetry could
61 offer a valuable tool that can assist with treatment individualisation. However, unlike
62 EBRT and brachytherapy, in MRT there is in general still a shortage of agreed
63 absorbed dose thresholds for lesions or absorbed dose constraints for organs at risk
64 (OARs) that could be prescribed. Well-designed studies aimed to provide robust
65 dosimetry and response data, and prospective trials to confirm the findings, are
66 therefore required to fully optimise therapies based on absorbed dose treatment
67 planning.

68 In cases where dosimetry is not directly employed to individualise a therapy, there is
69 still scope to use it to verify treatment delivery. Comparison of absorbed doses to that
70 of population data can be used for evaluating likely response or toxicity. While this is
71 of interest for all therapies, it may be particularly useful to inform a therapy with unusual
72 clinical indications or where treatment outcome or toxicity is of particular concern. ,In
73 such cases a patient could be selected for increased monitoring or observation.
74 Alternatively, it may be possible that additional cycles are stopped early, potentially
75 saving the health authority the expense of a costly treatment and allowing the patient
76 to move quickly to a more appropriate treatment strategy. This prospect for clinical
77 and economic benefit, must be weighed up against the additional cost of the dosimetry
78 and requires adequate dosimetry data available with which to compare and define a
79 “normal range”.

80 Evidently for the widespread clinical benefit of dosimetry to be fully implemented,
81 commitment from clinical centres to acquire and collate dosimetry data is required.
82 Without first gathering such data, population dose distributions cannot be derived, nor
83 “normal” ranges defined. Equally absorbed dose constraints and toxicity thresholds

84 cannot be evaluated to inform the design of the necessary randomised controlled trials
85 with which to definitively demonstrate improved efficacy.

86 In 2020 the EANM noted that interpretation of EC Directive 2013/59/Euratom, laying
87 down basic safety standards (BSS) for protection against the dangers arising from
88 exposure to ionizing radiation [14] into practical application was still lacking across
89 Europe. The EANM position statement proposed three different classes of treatment
90 verification and optimisation [15] inspired by the indication of levels in prescribing,
91 recording and reporting of absorbed doses after radiotherapy defined by the
92 International Commission on Radiation Units and Measurements (ICRU) and later
93 defined for radiopharmaceuticals in ICRU report 96 [16]. Recently, a joint EANM,
94 SNMMI and IAEA enabling guide on how to set-up a theranostics centre was released
95 [17, 18] advising centres on important considerations for delivering these therapies.
96 With the ever-increasing variety of therapies, there is also a wide range of dosimetry
97 methodologies available the integration of such approaches into a clinical service can
98 be daunting. The EANM have further conducted a survey evaluating the potential time
99 and personnel resources typically being dedicated to different aspects of dosimetry for
100 MRT [19]. These data provide a useful perspective for centres to understand the
101 practicality of the resource requirement for MRT dosimetry and explore methods of
102 reducing that burden where possible.

103

104 In this document we discuss the requirements for introducing dosimetry as part of the
105 theranostic procedure and argue how a dosimetry regimen can be tailored to the
106 available resources of a centre depending on the needs of the department, national
107 regulations and which of the dosimetry levels is being considered. The aim is to help

108 centres wishing to initiate a dosimetry service but may not have the experience or
109 resources of the more established therapy and dosimetry centres.

110 Making Dosimetry Accessible

111 Careful preparation is needed before a dosimetry service or study can commence.
112 This was highlighted in the EANM resource survey [19] which considered three
113 separate steps in implementing dosimetry: 1) protocol development; 2) preparatory
114 work; and finally 3) the patient studies.

115 Developing a dosimetry protocol

116 The EANM survey reported that the median time required to derive and develop a
117 clinical dosimetry protocol was 4 days. Appropriately, this process requires input from
118 different disciplines to ensure that the technical, clinical, and scientific aspects of the
119 protocol are met. The survey suggested that input from medical physics, NM
120 technologists and the medical practitioner was common. The EANM has an
121 established portfolio of both clinical and technical dosimetry guidelines produced by
122 multidisciplinary teams, and often prepared in conjunction with other international
123 organisations such as the IAEA, SNMMI and the MIRD committee. It remains the
124 ambition of the EANM to continue supporting the community in the production of these
125 guidelines and help in the formation of clear and appropriate operating procedures
126 related to dosimetry. Protocol choice will depend on the therapy, and the requirements
127 of department. Consideration should also be given as to the personal and medical
128 conditions of the patient, and protocols adjusted as necessary. Even for centres which
129 do not expect to deliver dosimetry-guided therapy, it is good practice to have such
130 systems of work in place in case a clinical case presents where verification and more
131 specialized treatment optimisation is required. Furthermore, dose-reporting to national

132 regulators in instances of accidental or unexpected exposure is usually a legislative
133 requirement that MRT centres must comply. In cases of unexpected early or late
134 toxicity effects, dosimetry documentation may help identifying or exclude possible
135 contributions or causes (e.g. specific/newly identified risk factors) related to certain
136 patients or specific clinical characteristics.

137 [Initial Preparations and System Configurations](#)

138 Prior to commencing a dosimetry study, it is often necessary to undertake some initial
139 preparatory work such as system commissioning, configuration, and testing. These
140 are generally required to obtain baseline or system characteristics and ensure the
141 developed protocol is suitable prior to first use. Methodologies for such studies are
142 well documented in the appropriate guidelines. Provided that the mandated regular
143 quality control assessments are fulfilled, the periodicity of the specific dosimetry tests
144 can be low (yearly, twice per year or quarterly). The most time intensive tests indicated
145 by the EANM survey were the imaging tests. Comparatively, resource requirements
146 for these are similar to that required on PET/CT systems for trial accreditation. For
147 dosimetry and therapeutic applications, the radionuclides used are of a considerably
148 longer half-life than positron emitters and therefore coordination of phantom
149 preparation is arguably much easier as more time can be given between source
150 preparation and scanning. There is also the added advantage that multiple gamma
151 cameras can be tested with the same phantom preparation, further reducing resource
152 requirements. Results from multi-centre comparison exercises and clinical trials have
153 also demonstrated consistent system characteristics across similar SPECT models
154 potentially negating the need to establish these for every system, provided similar
155 acquisition protocols are adopted [20, 21].

156 For non-imaging preparatory work including detector calibration, resources are
157 considerably less arduous and can very often be performed on a daily or patient basis.
158 For example, to determine a conversion factor between whole-body activity and dose-
159 rate measurements, a “self-calibration” technique consisting of a quick measurement
160 of a few minutes acquired immediately after administration (before any voiding), can
161 be used [22]. Conversely for other radiation detection systems, such as gamma well
162 counters or thyroid uptake probes, sensitivity should be measured at regular intervals.
163 Rather than undertaking complex phantom preparation each time, the sensitivity can
164 be checked initially with the therapeutic radionuclide and then regularly monitored with
165 a long-lived sealed source, such as that used for daily quality assurance of a dose
166 calibrator.

167 [Dosimetry Acquisitions and Calculations](#)

168 The EANM position paper on Directive 2013/59 proposed three levels of dosimetry
169 and the resource requirements for these levels can be tailored appropriately to suit the
170 clinical indication, the intent of the dosimetry and the resources of the department.
171 Thus, the first step is to decide the aim of the dosimetry. This will then influence the
172 required output (e.g. organs of interest) and the appropriate dosimetry method for that
173 therapy and centre. The accuracy of a dose estimate will inevitably decrease with
174 protocol simplifications (as outlined in the supplementary examples). However, this
175 may be acceptable in many clinical scenarios, and the dosimetric approach should be
176 guided based on the clinical need and acceptable level of uncertainty in dose estimate.

177 Dosimetry using patient cohort-averaged dose data requires very little resourcing
178 beyond collating the typical doses reported in the literature for the therapy in question.
179 This information can be gathered when first developing the therapy protocol and is

180 often readily available in the appropriate guidance documents. For most MRT
181 procedures, a range or distribution of absorbed doses have been reported, providing
182 valuable indication of the likeliness of potential under- or over-dosing in a population.
183 For an individual, cohort-based absorbed doses to pathologic and limiting tissues can
184 be estimated according to the activity administered with the treatment delivery
185 confirmed through post therapy imaging.

186 A personalized dose assessment following a therapy is often associated with the need
187 to acquire SPECT/CT studies at multiple time-points spanning many days. However,
188 significant work has been undertaken to validate practical methods to reduce the
189 burden to the patient and department [23]. For centres with reduced capacity when
190 delivering therapies over multiple cycles, dosimetry could be performed at alternate
191 cycles, or just on the initial cycle. Alternatively, when post therapy imaging is being
192 performed as part of level 1 verification, it is often not a substantial effort to develop
193 this into a quantitative image. A combination of the patient-specific quantitative
194 measurement with population effective half-lives can, for some MRT procedure and
195 organs, enable a population-based absorbed dose estimate based on a single time
196 point acquisition [24-26].

197 When camera availability is the limiting factor, multiple time-point SPECT acquisitions
198 can be replaced with a hybrid approach that uses a combination of SPECT/CT
199 complemented with less time consuming yet not fully quantitative planar or whole body
200 imaging [27, 28]. The planar data are used for temporal sampling and do not need to
201 be diagnostic quality, enabling further reduction in acquisition time. However, region-
202 based determination of uptake based on 2D projections is only possible for some
203 radiopharmaceuticals and pathologies (e.g., due to overlap of different regions of
204 interest in anteroposterior direction). In some cases, dosimetry evaluations can also

205 be performed without any imaging: noteworthy examples include thyroid uptake
206 measurements or whole-body dosimetry using external radiation detectors [29]. These
207 have the advantage that they do not impact camera availability.

208 Methods to reduce resource burden for verification can equally translate that required
209 for the prescription of an activity based on a desired absorbed dose. In a theranostic
210 setting, it is often standard practise to confirm patient eligibility with a diagnostic
211 conjugate of the therapeutic compound. There is therefore extensive interest in using
212 the pre-therapy images to predict therapeutic absorbed doses. This information could
213 be used to tailor the activity prescription to deliver an optimised therapeutic absorbed
214 dose and is an approach shown to be highly successful in SIRT [7]. Such methods
215 have particular relevance in view of possible dose escalation beyond standard
216 administered activity indications. Alternatively, with fractionated treatments, dosimetry
217 performed after an initial cycle can be used to adjust the activity or number of
218 subsequent cycles, which considerably reduces the “pre-therapy” dosimetry workload.
219 As with level 2, the method of dosimetry does not necessarily lead to a high burden,
220 as standard operating procedures using whole-body, blood based and thyroid probe
221 measurements are available for many treatments [5, 22, 24, 29, 30].

222 **Staff Requirements**

223 MRT dosimetry involves different competencies that must be present in a
224 multidisciplinary team including physicians, medical physicists and technologists. Staff
225 resourcing is a significant consideration when starting a dosimetry service. Dose
226 calculations should be performed and completed timely prior to any concerned
227 treatment. When scheduling times and resources, the time dedicated for data analysis
228 and dosimetry calculations should also be considered alongside that allocated for

229 physical measurements and scanning. The EANM survey indicated work-load times
230 required to process and analyse dosimetry data. It should be recognised that, for a
231 new service, many of these tasks may at first take longer, while converging to
232 improved time-efficiency as experience improves. Economy of scale will also help
233 reducing the impact on personnel. However, commitment to resourcing and
234 infrastructure remains usually the primary barrier to implementation of a dosimetry
235 service.

236 [Role of the medical physicist](#)

237 The BSS directive stipulates that a medical physics expert should act or give specialist
238 advice, as appropriate, on matters relating to radiation physics for implementing the
239 requirements set out in the directive. This includes taking responsibility for dosimetry,
240 including physical measurements for the therapeutic activity to administer to the
241 patient, estimation of absorbed doses and dose estimates to other personnel involved
242 in the therapeutic procedures. The EANM survey demonstrated that a medical
243 physicist was primarily involved in most aspects of the dosimetry chain but did not
244 differentiate between the experience and the level of qualification of that medical
245 physicist. In practical terms, many of the procedures required for dosimetry
246 calculations can be performed by a variety of staff, including junior medical physicists,
247 radiopharmacy lab technicians, nuclear medicine technologists, physicians, or nurses.
248 Where physics resources are scarce, it may be beneficial to explore options for shared
249 services and cross-site collaboration. Centralising tasks such as image processing
250 and analysis might enhance the efficiency of the dosimetry and promote the optimal
251 use of the local resources.

252 **Role of the physician**

253 The treating nuclear medicine physician having a comprehensive view of the patient
254 situation should have appropriate training to assess and evaluate the suitability and/or
255 the requirements for a dosimetrically optimised treatment. It should therefore be the
256 responsibility of the physician to identify suitable patients and interpret the clinical
257 significance of an absorbed dose, considering all patient clinical factors and other
258 biomarkers of response and toxicity. The practitioner is responsible for the prescribed
259 therapeutic activity and justifies the exposure to the patient, and therefore needs to be
260 fully engaged in the multidisciplinary team responsible for performing dosimetry.

261 In many European centres the nuclear medicine physician may also have a
262 managerial role in the running of the NM department and would therefore have a
263 clearer understanding of the resources and personnel available to commit to
264 dosimetry. In addition to this overarching authority, the physician can play an
265 important role in some of the practical aspects of the dosimetry regimen., such as
266 identification and segmentation of lesions and tissues of interest. Nevertheless, to
267 reduce the burden on the nuclear medicine physician, a multidisciplinary approach can
268 still be adopted, whereby the initial contouring is defined by a medical physicist, a NM
269 technologist or in a semi-automated fashion and later verified by the physician.

270 **Role of the nuclear medicine technologist**

271 The role of the NM technologist should not be underestimated when developing a
272 dosimetry service. In many countries, the NM technologist is the key person in
273 communication with the patient, often involved in making appointments, informing
274 them from the beginning and supporting the patient through the different dosimetry
275 examinations. A technologist will likely spend the most time with the patient during

276 intensive scanning regimens. Improving a patient's experience will result in better
277 patient cooperation and finally increase the quality of the exams. . For some dosimetry
278 procedures, the technologist may be responsible for taking samples (blood and urine)
279 and for manipulating the samples (e.g. well counter measurements) as necessary. The
280 NM technologist will likely also assist the medical physicist in maintaining quality
281 assurance of devices and procedures.

282 It is therefore essential that NM technologists are well trained in the dosimetry protocol
283 and feel involved and engaged in all aspects of their role. The NM technologist needs
284 to understand the rationale for dosimetry and the requirement for accurate data
285 collection. Good communication with the medical physicists and physicians is
286 therefore a key factor to ensure that dosimetry remains functional and practical.

287 **Optimising Equipment Resources**

288 Equipment is a valuable, costly and time limited resource within a nuclear medicine
289 department. The equipment required for dosimetry will vary depending on the specific
290 MRT protocol, which, in many cases, can be tailored to suit equipment availability.
291 This latter aspect is particularly sensible when first implementing dosimetry, negating
292 or minimizing the need for initial outlay costs. As the dosimetry service becomes more
293 established, protocols can always be further developed, and additional equipment
294 procured if necessary.

295 **External radiation monitors**

296 Hand held radiation monitors are a common piece of equipment and should be
297 available within any nuclear medicine department. Whole-body dosimetry
298 measurements can be made with almost any type of monitor, provided its response
299 has been characterised. If only being used occasionally, a monitor could temporarily

300 be brought to the patient. For regular use, it may be more appropriate to have a
301 dedicated system configured in the treatment facility, attached to a trolley or tripod, or
302 permanently fixed to the wall or ceiling, which can make patient positioning and
303 measurement more efficient and reproducible. In most cases, centres opt for bespoke
304 configurations to suit their individual needs, although commercial options, including
305 those with direct output to PCs are available.

306 [Gamma Counters](#)

307 Due to the low activity concentrations, blood based dosimetry generally requires
308 samples to be measured using a well-type NaI(Tl) detector (gamma counter) [22]. If
309 a department provides a GFR service or cisternography with [^{99m}Tc]-DTPA, this
310 equipment should be readily available. For therapeutic radionuclides in general, a
311 large flexibility exists in measuring samples at different time points without adversely
312 affecting other users of the gamma counter. For centres without such equipment, less
313 costly options could be built inhouse using a well shielded sodium iodine detector or if
314 available a high purity germanium (HPGe) detector. Radionuclide activity meters
315 (commonly known as dose calibrators) are generally only accurate down to a few
316 megabecquerels and are therefore insufficiently sensitive for the task. Therefore, in
317 some cases it is more sensible to pursue a different method of dosimetry rather than
318 purchase this equipment for dosimetry only. The EANM provide guidelines detailing
319 alternate methods of bone marrow dosimetry beyond that of blood sampling [22].

320 [Thyroid uptake probes](#)

321 Thyroid uptake probes consist of a thallium-activated sodium iodide crystal coupled to
322 a multiscale analyser or energy discriminator and counting system. The probe is
323 collimated with lead to give a field of view appropriate to cover the patient neck area.

324 Various dedicated commercial options exist, or a system could potentially be
325 constructed in-house if an appropriate detector is available. For centres without a
326 dedicated probe, gamma camera imaging may also be performed to provide the same
327 information. The need for a dedicated system is then a trade-off between purchase
328 cost and gamma camera capacity. While these systems are primarily designed to
329 measure uptake of I-123 or I-131 in the thyroid, they can also be used for other
330 measurements such as whole-body count rates or activity in blood samples. For such
331 alternative uses, the probe response would first need to be characterised to avoid
332 dead-time effects. In such cases, measurement of high-activity blood samples can be
333 delayed until sufficiently decayed.

334 **Imaging Equipment**

335 Most forms of image-based dosimetry are currently performed using gamma cameras
336 or SPECT systems. While SPECT/CT imaging is often recommended, it is, for several
337 applications, also possible to use methods based on SPECT only or planar gamma
338 camera imaging [24, 28]. It is evident that a centre providing a theranostic service
339 needs access to at least one gamma camera.

340 In general, patient scanning may require up to 2 hours of camera-time for individual
341 patients when multiple imaging sessions are performed [19]. However, reducing the
342 number of time-points appears feasible for some treatments, when the
343 pharmacokinetics are well described. Single time-point protocols have been
344 suggested for both [¹⁷⁷Lu]-DOTATATE kidney dosimetry and [¹⁷⁷Lu]-PSMA-617 [31,
345 32]. In the future, acquisition times could be reduced through technological
346 advancements such as the introduction of AI-based reconstruction protocols and
347 acceleration of SPECT/CT acquisition protocols [33].

348 Specific MRT applications exist for PET/CT used to directly image [⁹⁰Y]-microspheres
349 for post-therapy dosimetry verification after radioembolisation and some β^+ emitter
350 diagnostic companions included in the theragnostic workflow. Alternatives exist for
351 centres without PET scanners, in the form of the gamma camera based
352 bremsstrahlung imaging for ⁹⁰Y [34] or single photon emission based tracers such as
353 ¹¹¹In or ^{99m}Tc in place of ⁶⁸Ga [35]. It is worth noting that Bremsstrahlung imaging of
354 ⁹⁰Y is typically a non-quantitative procedure and less suited for accurate dosimetry,
355 but instead useful for qualitative treatment verification [34]. While anatomical
356 information is readily obtainable through the CT component of hybrid scanners,
357 extraction of volume measures or co-registration of images from e.g. standalone CTs
358 are also possible and a lack of CT should not be a barrier for a centre wishing to
359 perform dosimetry.

360 [Software](#)

361 When considering the entire dosimetry workflow, the image post-processing aspects
362 specifically required for the dose calculation typically takes up two thirds of the total
363 personnel resources time. For this reason, the selection and implementation of
364 software used for dosimetry is of great importance. Due to the absence of commercial
365 dosimetry software in the past, dosimetry calculations have long been relying on in-
366 house solutions. However, an increasing number of commercial dosimetry software
367 solutions have become available over the last years. Most are both CE marked and/or
368 FDA approved [36, 37], but very heterogeneous in function and application. The cost
369 of commercial dosimetry packages may require a large number of patients and
370 reimbursement to be cost-effective, and affordable to a department. Academic and
371 freeware software may therefore be an alternative option. For less advanced
372 calculations, it is often reasonable to employ basic image computing platforms for

373 viewing and segmentation, in combination with spreadsheets or freely available
374 general-purpose programming languages [38, 39]. The personnel effort required to
375 implement an academic or freeware-based solution is likely to be greater than for a
376 commercial software solution. However, the former offers more flexibility and allows
377 the users to develop a bespoke solution tailored to the individual centre. Provided
378 sufficient skills and knowledge of the user/developer are available. An adequate
379 internal benchmarking/validation system should be developed.

380 Discussion

381 The field of MRT is rapidly evolving and expanding its clinical prominence to multiple
382 new tumour entities [40]. The approval of ¹⁷⁷Lu-PSMA 617 by FDA and EMA
383 manifests the successful expansion of MRT to a high-volume indication such as
384 metastatic castration resistant prostate cancer. The pivotal trial (VISION) leading to
385 approval used a standard activity (7.4 GBq) in four and up to six cycles of ¹⁷⁷Lu-
386 PSMA 617 confirming a median overall survival and median progression free survival
387 benefit of 4,0 and 5,3 months compared to the SOC group, [41]. However, more than
388 50% of patients in the treatment arm did not achieve a PSA decrease of >50%. In
389 consideration of an overall well tolerated one size fits all dosing approach it can be
390 discussed if a more personalized approach taking advantage of a large therapeutic
391 window might increase the rate of responders. The currently ongoing read out of the
392 VISION dosimetry sub-study will provide information how the therapeutic activities can
393 be individually escalated when based on normal organ doses as well as provide intel
394 on achievable (and required) tumour doses. An improvement in response and more
395 importantly survival would clearly justify the added effort, cost and exposure of
396 dosimetry to patients, medical experts and society.

397 In the wake of an ever-increasing number of new MRT programs and a better
398 understanding of radiobiology [42] dosimetry has the opportunity especially in early
399 phases of clinical development to fast-track clinical translation, improve the
400 understanding of a potential therapeutic index, and reduce the risk of late phase
401 clinical trial failures.

402 Conclusions

403 Dosimetry plays a key role in the personalisation and continued optimisation of
404 theragnostic nuclear medicine. Procedures to implement dosimetry can be optimised
405 to suit the needs and resources of the department.

- 407 1. Chiesa, C., et al., *A dosimetric treatment planning strategy in radioembolization*
408 *of hepatocarcinoma with Y-90 glass microspheres*. Quarterly Journal of Nuclear
409 Medicine and Molecular Imaging, 2012. **56**(6): p. 503-508.
- 410 2. Del Prete, M., F.A. Buteau, and J.M. Beaugregard, *Personalized Lu-177-*
411 *octreotate peptide receptor radionuclide therapy of neuroendocrine tumours: a*
412 *simulation study*. European Journal of Nuclear Medicine and Molecular
413 Imaging, 2017. **44**(9): p. 1490-1500.
- 414 3. Maxon, H.R., et al., *Radioiodine-131 Therapy for Well-Differentiated Thyroid-*
415 *Cancer - a Quantitative Radiation Dosimetric Approach - Outcome and*
416 *Validation in 85 Patients*. Journal of Nuclear Medicine, 1992. **33**(6): p. 1132-
417 1136.
- 418 4. Sandstrom, M., et al., *Individualized Dosimetry of Kidney and Bone Marrow in*
419 *Patients Undergoing Lu-177-DOTA-Octreotate Treatment*. Journal of Nuclear
420 Medicine, 2013. **54**(1): p. 33-41.
- 421 5. Stokkel, M.P.M., et al., *EANM procedure guidelines for therapy of benign*
422 *thyroid disease*. European Journal of Nuclear Medicine and Molecular Imaging,
423 2010. **37**(11): p. 2218-2228.
- 424 6. Strigari, L., et al., *The evidence base for the use of internal dosimetry in the*
425 *clinical practice of molecular radiotherapy*. European Journal of Nuclear
426 Medicine and Molecular Imaging, 2014. **41**(10): p. 1976-1988.
- 427 7. Garin, E., et al., *Personalised versus standard dosimetry approach of selective*
428 *internal radiation therapy in patients with locally advanced hepatocellular*
429 *carcinoma (DOSISPHERE-01): a randomised, multicentre, open-label phase 2*
430 *trial*. Lancet Gastroenterology & Hepatology, 2021. **6**(1): p. 17-29.
- 431 8. Garske-Roman, U., et al., *Prospective observational study of Lu-177-DOTA-*
432 *octreotate therapy in 200 patients with advanced metastasized neuroendocrine*
433 *tumours (NETs): feasibility and impact of a dosimetry-guided study protocol on*
434 *outcome and toxicity*. European Journal of Nuclear Medicine and Molecular
435 Imaging, 2018. **45**(6): p. 970-988.
- 436 9. Allimant, C., et al., *Tumor Targeting and Three-Dimensional Voxel-Based*
437 *Dosimetry to Predict Tumor Response, Toxicity, and Survival after Yttrium-90*
438 *Resin Microsphere Radioembolization in Hepatocellular Carcinoma*. Journal of
439 Vascular and Interventional Radiology, 2018. **29**(12): p. 1662-1670.
- 440 10. Cremonesi, M., et al., *Correlation of dose with toxicity and tumour response to*
441 *Y-90- and Lu-177-PRRT provides the basis for optimization through*
442 *individualized treatment planning*. European Journal of Nuclear Medicine and
443 Molecular Imaging, 2018. **45**(13): p. 2426-2441.
- 444 11. Del Prete, M., et al., *Personalized Lu-177-octreotate peptide receptor*
445 *radionuclide therapy of neuroendocrine tumours: initial results from the P-*
446 *PRRT trial*. European Journal of Nuclear Medicine and Molecular Imaging,
447 2019. **46**(3): p. 728-742.
- 448 12. Dewaraja, Y.K., et al., *Tumor-Absorbed Dose Predicts Progression-Free*
449 *Survival Following I-131-Tositumomab Radioimmunotherapy*. Journal of
450 Nuclear Medicine, 2014. **55**(7): p. 1047-1053.
- 451 13. Levillain, H., et al., *International recommendations for personalised selective*
452 *internal radiation therapy of primary and metastatic liver diseases with yttrium-*

- 453 90 resin microspheres. *European Journal of Nuclear Medicine and Molecular*
454 *Imaging*, 2021. **48**(5): p. 1570-1584.
- 455 14. *Council Directive 2013/59/Euratom*. . Official Journal of the European Union,
456 2013. **56**.
- 457 15. Konijnenberg, M., et al., *EANM position paper on article 56 of the Council*
458 *Directive 2013/59/Euratom (basic safety standards) for nuclear medicine*
459 *therapy*. *Eur J Nucl Med Mol Imaging*, 2021. **48**(1): p. 67-72.
- 460 16. Sgouros, G., et al., *ICRU Report 96, Dosimetry-Guided Radiopharmaceutical*
461 *Therapy*, in *Journal of the ICRU*. 2022, THE INTERNATIONAL COMMISSION
462 ON RADIATION UNITS AND MEASUREMENTS.
- 463 17. Herrmann, K., et al., *Joint EANM, SNMMI and IAEA enabling guide: how to set*
464 *up a theranostics centre*. *European Journal of Nuclear Medicine and Molecular*
465 *Imaging*, 2022. **49**(7): p. 2300-2309.
- 466 18. Herrmann, K., et al., *Joint EANM, SNMMI and IAEA Enabling Guide: How to*
467 *Set Up a Theranostics Centre*. *Journal of Nuclear Medicine*, 2022: p.
468 jnumed.122.264321.
- 469 19. Gabiña, P.M., et al., *Results From A Survey On Time Estimates And Personnel*
470 *Responsible For Main Tasks In Molecular Radiotherapy Dosimetry*. IN PRESS.
- 471 20. Taprogge, J., F. Leek, and G.D. Flux, *Physics aspects of setting up a*
472 *multicenter clinical trial involving internal dosimetry of radioiodine treatment of*
473 *differentiated thyroid cancer*. *Quarterly Journal of Nuclear Medicine and*
474 *Molecular Imaging*, 2019. **63**(3): p. 271-277.
- 475 21. Tran-Gia, J., et al., *A multicentre and multi-national evaluation of the accuracy*
476 *of quantitative Lu-177 SPECT/CT imaging performed within the MRT Dosimetry*
477 *project*. *Ejnm Physics*, 2021. **8**(1).
- 478 22. Hindorf, C., et al., *EANM Dosimetry Committee guidelines for bone marrow and*
479 *whole-body dosimetry*. *European Journal of Nuclear Medicine and Molecular*
480 *Imaging*, 2010. **37**(6): p. 1238-1250.
- 481 23. Ligonnet, T., et al., *Simplified patient-specific renal dosimetry in Lu-177 therapy:*
482 *a proof of concept*. *Physica Medica-European Journal of Medical Physics*,
483 2021. **92**: p. 75-85.
- 484 24. Hanscheid, H., et al., *EANM Dosimetry Committee Series on Standard*
485 *Operational Procedures for Pre-Therapeutic Dosimetry II. Dosimetry prior to*
486 *radioiodine therapy of benign thyroid diseases*. *European Journal of Nuclear*
487 *Medicine and Molecular Imaging*, 2013. **40**(7): p. 1126-1134.
- 488 25. Hanscheid, H., et al., *Absorbed dose estimates from a single measurement one*
489 *to three days after the administration of Lu-177-DOTATATE/-TOC*.
490 *Nuklearmedizin-Nuclear Medicine*, 2017. **56**(6): p. 219-224.
- 491 26. Sundlov, A., et al., *Feasibility of simplifying renal dosimetry in Lu-177 peptide*
492 *receptor radionuclide therapy*. *Ejnm Physics*, 2018. **5**.
- 493 27. Ljungberg, M., et al., *MIRD Pamphlet No. 26: Joint EANM/MIRD Guidelines for*
494 *Quantitative Lu-177 SPECT Applied for Dosimetry of Radiopharmaceutical*
495 *Therapy*. *Journal of Nuclear Medicine*, 2016. **57**(1): p. 151-162.
- 496 28. Gleisner, K.S., et al., *EANM dosimetry committee recommendations for*
497 *dosimetry of 177Lu-labelled somatostatin-receptor- and PSMA-targeting*
498 *ligands*. *European Journal of Nuclear Medicine and Molecular Imaging*, 2022.
499 **49**(6): p. 1778-1809.
- 500 29. Gear, J., et al., *EANM Dosimetry Committee series on standard operational*
501 *procedures for internal dosimetry for I-131 mIBG treatment of neuroendocrine*
502 *tumours*. *Ejnm Physics*, 2020. **7**(1).

- 503 30. Lassmann, M., et al., *EANM Dosimetry Committee series on standard*
504 *operational rocedures for pre-therapeutic dosimetry I: blood and bone marrow*
505 *dosimetry in differentiated thyroid cancer therapy*. European Journal of Nuclear
506 Medicine and Molecular Imaging, 2008. **35**(7): p. 1405-1412.
- 507 31. Hanscheid, H., et al., *Dose Mapping After Endoradiotherapy with Lu-177-*
508 *DOTATATE/DOTATOC by a Single Measurement After 4 Days*. Journal of
509 Nuclear Medicine, 2018. **59**(1): p. 75-81.
- 510 32. Jackson, P.A., et al., *Radiation Dosimetry in Lu-177-PSMA-617 Therapy Using*
511 *a Single Posttreatment SPECT/CT Scan: A Novel Methodology to Generate*
512 *Time- and Tissue-Specific Dose Factors*. Journal of Nuclear Medicine, 2020.
513 **61**(7): p. 1030-1036.
- 514 33. Ryden, T., et al., *Deep-Learning Generation of Synthetic Intermediate*
515 *Projections Improves Lu-177 SPECT Images Reconstructed with Sparsely*
516 *Acquired Projections*. Journal of Nuclear Medicine, 2021. **62**(4): p. 528-535.
- 517 34. Chiesa, C., et al., *EANM dosimetry committee series on standard operational*
518 *procedures: a unified methodology for Tc-99m-MAA pre- and Y-90 peri-therapy*
519 *dosimetry in liver radioembolization with Y-90 microspheres*. Ejnmmi Physics,
520 2021. **8**(1).
- 521 35. Deppen, S.A., et al., *Ga-68-DOTATATE Compared with In-111-DTPA-*
522 *Octreotide and Conventional Imaging for Pulmonary and*
523 *Gastroenteropancreatic Neuroendocrine Tumors: A Systematic Review and*
524 *Meta-Analysis*. Journal of Nuclear Medicine, 2016. **57**(6): p. 872-878.
- 525 36. Della Gala, G., et al., *Overview of commercial treatment planning systems for*
526 *targeted radionuclide therapy*. Phys Med, 2021. **92**: p. 52-61.
- 527 37. Mora-Ramirez, E., et al., *Comparison of commercial dosimetric software*
528 *platforms in patients treated with Lu-177-DOTATATE for peptide receptor*
529 *radionuclide therapy*. Medical Physics, 2020. **47**(9): p. 4602-4615.
- 530 38. Fedorov, A., et al., *3D Slicer as an image computing platform for the*
531 *Quantitative Imaging Network*. Magn Reson Imaging, 2012. **30**(9): p. 1323-41.
- 532 39. Schindelin, J., et al., *Fiji: an open-source platform for biological-image analysis*.
533 Nature Methods, 2012. **9**(7): p. 676-682.
- 534 40. Bodei, L., et al., *Radiotheranostics in oncology: current challenges and*
535 *emerging opportunities*. Nat Rev Clin Oncol, 2022. **19**(8): p. 534-550.
- 536 41. Sartor, O., et al., *Lutetium-177-PSMA-617 for Metastatic Castration-Resistant*
537 *Prostate Cancer*. N Engl J Med, 2021. **385**(12): p. 1091-1103.
- 538 42. Pouget, J.P., et al., *An EANM position paper on advancing radiobiology for*
539 *shaping the future of nuclear medicine*. Eur J Nucl Med Mol Imaging, 2023.
540 **50**(2): p. 242-246.

541 Statements and Declarations

542 Funding

543 NHS funding was provided to the NIHR Biomedical Research Centre at The Royal

544 Marsden and the ICR

545 **Competing Interests**

546 KH reports personal fees from Bayer, personal fees and other from Sofie Biosciences,
547 personal fees from SIRTEX, non-financial support from ABX, personal fees from
548 Adacap, personal fees from Curium, personal fees from Endocyte, grants and
549 personal fees from BTG, personal fees from IPSEN, personal fees from Siemens
550 Healthineers, personal fees from GE Healthcare, personal fees from Amgen, personal
551 fees from Novartis, personal fees from ymabs, all outside the submitted work. LG
552 reports personal fees from Roche Diagnostics and SNIBE for advisory board
553 participation, and research support from Roche Diagnostics., all outside the submitted
554 work.

555 **Ethics Approval**

556 This manuscript does not contain proprietary research involving either humans or
557 animals

558 **Consent to Participate**

559 This manuscript does not contain proprietary human data; accordingly an informed
560 consent is not applicable.

561 **Liability**

562 This guide summarizes the views of the co-authoring EANM Committee members. It
563 reflects recommendations for which the EANM cannot be held responsible. The
564 recommendations should be taken into the context of good practice of nuclear
565 medicine and do not substitute for national and international legal or regulatory
566 provisions.

567